New solid-state organic membrane based lead-selective micro-electrode

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Abstract

Microfabrication, characterization and analytical application of a new thin-film organic membrane based lead-selective micro-electrode have been elaborated. Prior to the fabrication of the assembly, the gold thin-film substrate has been electrochemically treated using a new technique. The developed micro-electrode based on *tert*-Butylcalix[4]arene-tetrakis(N,N-dimethylthioacetamide) as electroactive sensing material, carboxylated PVC as supporting matrix, 2-nitrophenyl octyl ether as solvent mediator and potassium tetrakiss (4-chlorophenyl) borate as lipophilic additive, respectively, provides a nearly Nernstian response (slope 28 ± 0.5 mV/concentration decade) covering the concentration range $1\times10^{-6} - 1\times10^{-2}$ mole L^{-1} of Pb(II) ions with reasonable selectivity over some tested cations. The merits offered by the new microelectrode include simple fabrication, low cost as well as automation and integration feasibility. Moreover, the suggested microelectrode has been successfully applied for the determination of lead ions in some aqueous samples. These samples were also determined using inductively coupled plasma atomic emission spectroscopy (ICP-AES) for comparison. The proposed electrode offers a good accuracy (the average recovery was 95.5%), high precision (RSD was <3%), fast response time (<30 s.) and long life span (>4 months).
Keywords: all-solid-state microelectrode, thin-film, substrate surface treatment, organic membrane, lead determination.

1 Introduction

Ion-selective electrodes (ISEs) and potentiometric sensors are the most widely used sensor types for the measurement of toxic heavy metal ions [1, 2]. The development of all-solid-state micro-sensor devices originating from potentiometric sensors has accelerated during the last few years, and this is likely to continue. The realization of such devices seems to be accelerating as micro-scale construction makes it possible to apply principles that would not work in macro-scale analogous. In addition, accurate and reliable analysis using miniaturized chemical sensors is a very useful analytical technique because of the avoidance of laborious and time consuming preliminary sample treatment. Moreover, micro-scale analyses of chemical species have many advantages over conventional methodologies, including high spatial resolution, rapid response, and minimal disturbance of the analyzed substrate [3]. Use of different organic and inorganic sensing materials with versatile properties in fabrication of all-solid-state micro-electrodes makes them suitable for the detection of many chemical species in solution at concentrations lying in the ppm range [4–10]. In realization of such devices, chalcogenide glasses were proven to be very promising ion-selective membranes especially for the detection of heavy metals in solution (Pb^{2+}, Cd^{2+}, Fe^{2+}, Cu^{2+}, Ag^+...) [4–6]. However, organic membrane-sensitive layers prepared on transducers, fabricated using different, less or more complicated and expensive, technologies for measurements of potassium [7] and lead [8] have been reported, too. In addition, nanoparticle labels (i.e., gold nanoparticles, silver tags, and semiconductor nanocrystals) have been used in the fabrication of potentiometric micro-sensors for detection of DNA hybridization [9] and carbon dioxide [10]. Miniaturization of solid-electrolyte gas sensors to thin-film micro-devices have been discussed in literature [11]. Microfabrication of chemical sensors and biosensors [12] as well as ISFET-based micro-sensors [13] for environmental monitoring has been reviewed. A Pt-Ir wire-based ISE has been suggested for monitoring the local spatial distribution of magnesium, pH and ionic currents [14]. Moreover, the realization of micro-sensors, based on a "lab-on-a-chip" has also been reviewed [15].

On the other hand, the development of organic membrane based micro-sensors has been recently introduced to overcome the low selectivity of chalcogenide glass and inorganic based thin-film micro-sensors [16–19]. However, there is an additional problem arise that the adhesion of the organic membrane to the thin-film substrate is usually poor, which produces an early degradation of those micro-sensors. To solve this problem, we had recently developed a new approach (Arida Approach) for the organic-based sensors micro-fabrications [17–19]. In this technique, the organic membrane-based sensitive layer has been nebulized in combination with a substrate surface treatment. Using these two steps in combination has distinctly improved the adhesion on the wafer surface. It decreases the leaching out of the ionophore and plasticizer, stabilizes the organic membrane, and consequently increases the micro-electrode's life-time.

In this paper, we describe the fabrication and characterization of PVC membrane-based micro-sensors using *tert*-Butylcalix[4]arene-tetrakis(N,N-dimethylthioacetamide) as lead ionophore [20], deposited on gold thin-film silicon micro-chips by the nebulization technique in combination with substrate surface treatment. The reliability of the suggested micro-sized lead sensors in comparison to independent standard methods using ICP-AES has been assessed.

2   Experimental

2.1 Chemicals and apparatus

The solvent mediator, 2-nitrophenyl octyl ether and the lipophylic additive potassium tetrakis(4-chlorophenyl) borate were purchased from Sigma-Aldrich (CH-9471 Buchs, Switzerland). The membrane support matrix, high molecular weight (220,000) poly(vinylchloride) carboxylated and the membrane solvent, THF (tetrahydrofurane) were purchased from Riedel-de Haën Chemical Company (Germany). The lead ionophore used was tert-Butylcalix[4]arene-tetrakis(N,N-dimethylthio-acetamide) (15343) purchased from Sigma-Aldrich chemical company. All the standard solutions of cations were prepared from their analytical reagent grade chemicals in deionized water, and then diluted to the desired concentration. Nitrate or chloride salts of the metal used were purchased from Riedel-de Haën. High purity standards (2% HNO_3, Pb 1000 mg kg^{-1}) were used for ICP-AES validation measurements after appropriate dilution with deionized water. Deionized water with conductivity <0.2 µS/cm used in the preparation and dilution of the reagents was produced using a Millipore Deionizer (Millipore, France, Elix 10).

The potentiometric measurements were performed at $20^{o}C$ with a HANNA microprocessor pH/ion analyzer (Model pH 211) using a thin-film lead micro-electrode in conjunction with a double-junction reference electrode immersed in stirred test solutions. The response characteristics and the selectivity coefficient $K_{Pb,M}^{pot}$ (obtained by separate solution method) of the thin-film lead micro-electrode have been measured using standard methods [21].

The morphology of the substrate surface was studied using a JEOL scanning electron microscope SEM (Model JSM 6390, Japan). A Perkin-Elmer (Optima 2100 DV) inductively coupled plasma atomic emission spectrometer (ICP-AES) instrument connected with an AS 93 Plus autosampler has been used for the standard determination of lead. The 40-MHz free-running generator was operated at a forward power of 1300 W; the outer, intermediate and Ar carrier gas flow rates were 15.0, 0.2 and 0.8 L/min, respectively. The pump flow rate was 1.5 mL/min. The carrier gas flow rate was optimized to obtain maximum signal-to-background ratios.

2.2 Micro-fabrication of the lead solid-state micro-electrode

A cocktail-coating mixture incorporating the Pb^{2+} ionophore was utilized as organic membrane-sensitive layer. The stock solution of this mixture was

prepared by mixing thoroughly 33 mg of powdered PVC, 57 mg of 2-nitrophenyl octyl ether plasticizer, 3 mg of potassium tetrakis (p-chlorophenyl) borate anion excluder and 7 mg of *tert*-Butylcalix[4]arene-tetrakis(N,N-dimethylthioacetamide) lead (II) ionophore in a small beaker. The mixture was then completely dissolved in 5 mL THF [16–19]. The sensor chips with the thin-film gold substrates were fabricated at Research Centre Jülich as described elsewhere [16, 22–24].

Prior to the deposition of ion-sensitive organic membrane, the gold thin-film substrate surface was treated electrochemically to enhance the adhesion to the organic membrane. Here, thin films of Ag precipitates have been deposited on the substrate surfaces from 10^{-3} mol L^{-1} $AgNO_3$ solution for 1 h using a home-made small electro-deposition cell. In combination with this step and based on the previously reported technique [17–19], the cocktail-coating mixture was nebulized on the treated surface of the gold thin-film substrate using a small commercial nebulizer. The nebulized solution was delivered to the substrate in fast pulses with 2 min intervals between the pulses. The deposition time was 30 min. After deposition of the organic membrane-sensitive layer, the sensors were scribed to single chips, glued and contacted via bonding to a printed circuit board (PCB) and encapsulated.

3   Results and discussion

3.1 Physical characterization of the lead micro-electrode

Using the nebulization method, the all-solid-state micro-electrode has been fabricated by depositing the organic membrane sensitive-layer on the treated surface of the silicon micro-chips (10 mm× 10 mm) and tested as lead-sensitive electrode. A video-microscopic picture of the organic membrane-based thin-film micro-electrode after integration into a PCB is shown in Fig. 1. The diameter of the thin-film micro-electrode is about 2 mm.
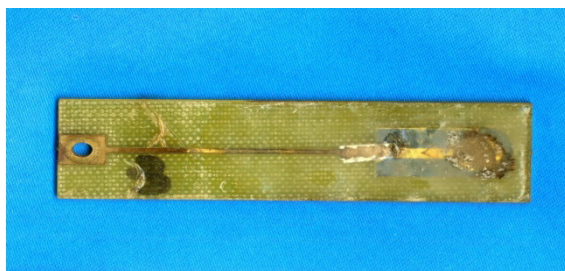

Figure 1:   Video-microscopic picture of an all-solid state lead micro-electrode.

Prior to the electrochemical characterization, the morphology studies on the gold thin-film substrate, treated substrate surface and organic membrane deposit have been performed using scanning electron microscopy (SEM) in order to check the film/membrane interface. The micrographs obtained are shown in

Fig. 2. The surfaces of all films do not present any observable defects. While, the untreated film (*a*) appears smooth and luster with poor adhesive properties, the treated substrate surface (*b*) becomes more mountain-like with high roughness and consequently, good adhesion to the organic membrane. The organic membrane film (*c*) is textured, homogenous and uniformly distributed. This significantly enhances the stability and consequently, the life span of the suggested micro-electrode.
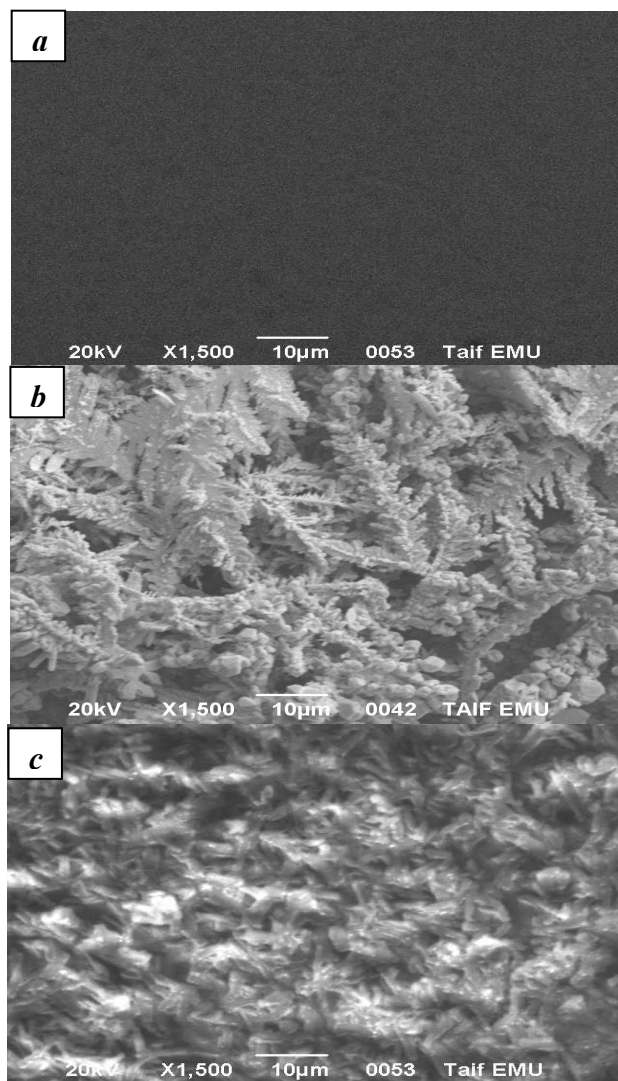

Figure 2:   SEM micrograph of the thin-film surfaces; (*a*) untreated gold substrate, (*b*) electrochemical treated and (*c*) nebulized organic membrane-sensitive layer.

3.2 Electrochemical evaluation of the lead micro-electrode

Our goal was to realize sensitive, stable and reliable all-solid-state lead micro-electrodes using the commercialized tert-Butylcalix[4]arene-tetrakis(N,N-dimethylthio-acetamide) lead ionophore. The suggested micro-electrode incorporating this ionophore has been electrochemically evaluated according to IUPAC recommendations in terms of sensitivity, stability, selectivity and reliability. In order to assess the reliability of the suggested micro-electrode, its response properties were compared with those reported for the bulk macro-electrode prepared by the same ionophore [20]. The data obtained are collected in Table 1. As can be seen, the micro-electrode showed a nearly theoretical Nernstian response (slope of 28±0.5 mV/concentration decade) with a straight line between 1×10^{-6} and 1×10^{-2} mole L^{-1} of Pb(II) ions (see Fig. 3). The limit of detection determined from the intersection of the two extrapolated segments of the calibration, as recommended by IUPAC, was 5×10^{-7} mol L^{-1}.

Table 1: Potentiometric performance properties of the thin-film lead micro-electrode and the bulk macro-electrode.

Parameter	All-solid-state thin-film micro-electrode	*Lead bulk macro-electrode
Slope (mV/decade)	28±0.5	28.7
Response time $t_{95\%}$(s)	<30	<10
Linear range (mol L^{-1})	1×10^{-2}-1×10^{-6}	1×10^{-2}-1×10^{-6}
Detection limit (mol L^{-1})	5×10^{-7}	3.2×10^{-7}
pH	2.2-6.3	3-6
Life span (months)	>4	<2

*Lead bulk macro-electrode [Ref. 20].

The response time and life span of an electrode are important features for analytical applications. Hence, the potentials of the suggested micro-electrode corresponding to four decade additions of Pb^{2+}, starting from deionized water to 10^{-2} mol L^{-1} have been measured. The results obtained are presented in Fig. 4. The response time ($t_{95\%}$) of the suggested micro-electrode in the whole linear concentration range was about 30 s. The stability and lifetime of the lead micro-electrode were also investigated by repeated calibrations at every two or three days for more than four months. During this period, the response time, slope and linear range are reproducible. Hence, the micro-electrode can be used for at least four months with practically unimpaired performance. Moreover, the suggested micro-electrode properties are almost similar or even somewhat better (life span) than the results observed for the lead macro-electrode based on the same ionophore [20]. The recently developed, nebulization technique of the organic membrane-sensitive layer in combination with the electrochemical treatment of the substrate surface significantly improves the adhesive properties of the membrane to the substrate surface, decreases the leaching out of the ionophore and plasticizer, stabilizes the organic membrane, and consequently increases the micro-electrodes' life-time (4> months).
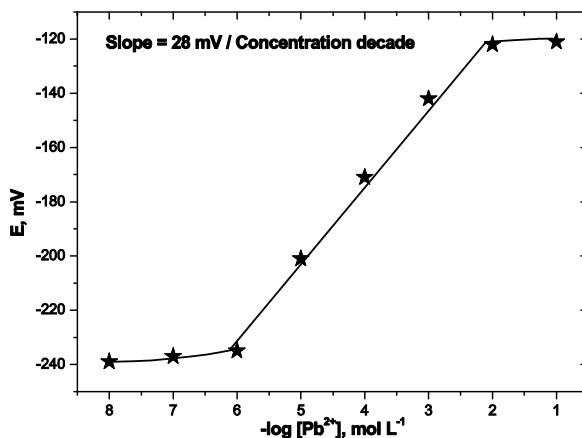
Figure 3:   Potentiometric calibration response of the organic membrane based lead microelectrode.
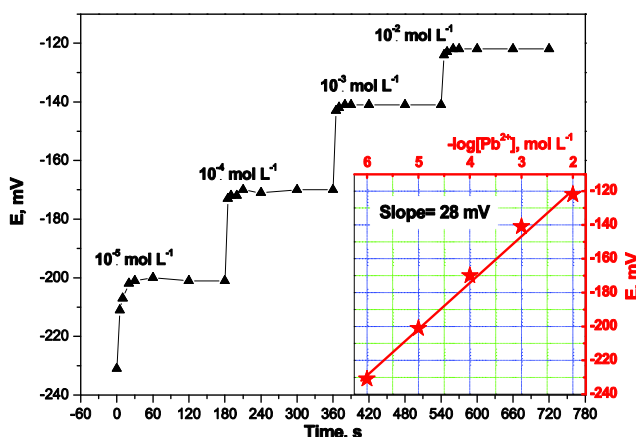

Figure 4:   Potentiometric dynamic response of the organic membrane based lead microelectrode.

The dependence of the response of the suggested micro-electrode on the pH value of the test solution was examined at two Pb^{2+} concentrations over the pH range between 1 and 8. As illustrated in Fig. 5, for both 1.0×10^{-3} and 1.0×10^{-2} mol L^{-1} Pb^{2+}, the potential remains constant over the pH range from pH 2.2 to 6.3. As a result, this range can be taken as the working pH range of the suggested micro-electrode. Variation of the potential at pH< 2 could be related to abundant H^+ ions which can protonate the ionophore in the membrane phase, resulting in its decomplexation of Pb^{2+}. While, decreasing of the potential at higher pH values may be ascribed to the hydrolysis of Pb^{2+} ions, leading to a decrease in its concentration.
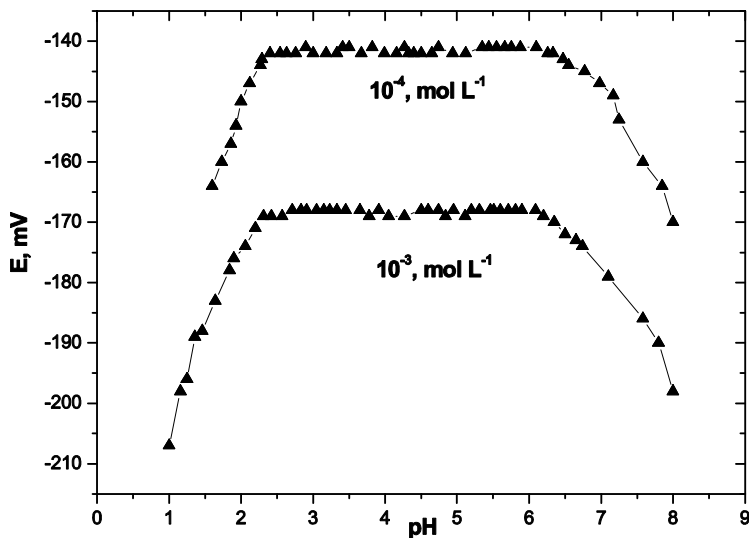
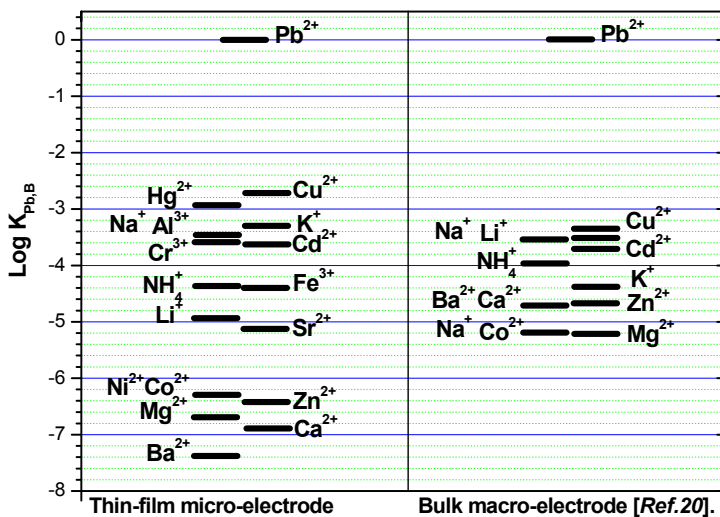Figure 5: Effect of pH on the potentionetric response of the organic membrane based lead microelectrode.

Figure 6: Selectivity coefficients, log $K_{Pb,B}$, for organic lead macro- and micro-electrodes, [0.01 mol L^{-1} of Pb$^+$ and interfering cations].

Potentiometric selectivity reflects the relative response of the membrane electrode for the primary ion over other ions, present in solution. This feature is perhaps the most important characteristics, since our goal here is the realization of a highly selective organic membrane-based lead micro-electrode instead of inorganic-based micro-sensors with high cross-sensitivity. The potentiometric response of the lead micro-electrode was studied in presence of some alkali, alkaline earth, transition metals, aluminum and ammonium ions. The potentiometric selectivity coefficients $K_{Pb,B}^{pot}$ were determined using the separate solution method [21]. The results depicted in Fig. 6 are compared with those reported for the bulk lead macro-electrode prepared with the same ionophore [20]. The data revealed that the suggested micro-electrode showed a very high selectivity towards most of the tested ions. This behavior is similar to or even more selective (Ba^{2+}, Ca^{2+}, Zn^{2+}, Mg^{2+}, Co^{2+} and Ni^{2+}) than values obtained from the macro-electrode based on the same ionophore. One possible explanation might be that the response mechanism of the micro-sized electrodes (particularly selectivity) is significantly affected by the size (surface to volume) effect. The enhancement of the micro-electrode' selectivity may be attributed to the fact that these chips have a large size to volume ratio as well as they offer a high density of electronic component and interconnection possibilities in contrast with the macro-electrodes based on the same ionophore.

3.3 Analytical applications of the proposed micro-electrode

To assess the applicability of the micro-electrode to lead measurements, an attempt was made to determine lead in five different samples under optimized conditions**.** These samples were also determined by an independent standard method using ICP-AES, for comparison. The data obtained are summarized in Table 2. As can be seen, there are no significant differences between the results obtained with the proposed micro-electrode and the reference method. In short, the results reveal a high accuracy (recovery 95.5%) and good reproducibility (RSD<3%, n=6).

Table 2:   Determination of lead in some aqueous samples employing the micro-electrode in comparison to the reference method ICP-AES.

No.	ICP-AES (mg/L)	*Thin-film micro-electrode (mg/L)	*Recovery %
1	0.21	0.22	104.7
2	5.23	4.88	93.3
3	25.67	23.78	92.6
4	93.01	86.11	92.5
5	210.64	199.57	94.7
Average	recovery		95.5

*The data is a mean of n= measurements.

4   Conclusion

A new thin-film organic membrane-based lead micro-electrode incorporating *tert*-Butylcalix[4]arene-tetrakis(N,N-dimethylthioacetamide) as electroactive material in a PVC matrix has been realized. The micro-electrode responds to lead ions in a nearly Nernstian behavior and presents a good selectivity and detection limit. The micro-electrode reveals a fast response time and long-term stability. It has been successfully applied for the determination of lead in some aqueous samples. The micro-electrode showed a good accuracy and reproducibility in comparison to the independent ICP-AES method.

Acknowledgement

References

[1]   Eric, B. & Ernö, P., Potentiometric sensors for trace-level analysis. *Trends in Analytical Chemistry*, 24(3), pp. 199-207, 2005.

[2]   Ru-Qin, Y., Zong-Rang, Z., Guo-Li S., Potentiometric sensors: aspects of the recent development. *Sensors and Actuators B: Chemical*, 65(1-3), pp. 150-153, 2000.

[3]   Wróblewski, W., Dybko, A., Malinowska, E., Brzózka, Z., Towards advanced chemical microsensors—an overview. *Talanta,* 63, pp. 33–39, 2004.

[4]   Taillades, G., Valls, O., Bratov, A., Dominguez, C., Pradel, A., Ribes, M.,ISE and ISFET microsensors based on a sensitive chalcogenide glass for copper ion detection in solution. *Sensors and Actuators B*, 59, pp. 123–127, 1999.

[5]   Guessous , A., Sarradin, J., Papet, P., Elkacemi, K., Belcadi, S., Pradel, A., Ribes, M., Chemical microsensors based on chalcogenide glasses for the detection of cadmium ions in solution. *Sensors and Actuators B,* 53, pp. 13– 18, 1998.

[6]   Schöning, M.J. & Kloock, J.P., About 20 Years of Silicon-Based Thin Film Sensors with Chalcogenide Glass Materials for Heavy Metal Analysis: Technological Aspects of Fabrication and Miniaturization- A review. *Electroanalysis*, 19, pp. 2029-2038, 2007.

[7]   Zachara, J. & Wróblewski, W., Design and performance of some microflow-cell potentiometric transducers. *Analyst*, 128, pp. 532–536, 2003.

[8]   ISILDAK, I., All Solid-State Contact Lead(II) Ion-selective PVC Membrane Electrode Using Dimethylene Bis(4-methylpiperidinedithiocarbamate) Neutral Ionophore. *Turk J Chem*, 24, pp. 389-394, 2000.

[9]   Numnuam, A., Chumbimuni-Torres, K.Y., Xiang, Y., Bash, R., Thavarungkul, P., Kanatharana, P., Pretsch, E., Wang, J., Bakker, E., Potentiometric Detection of DNA Hybridization. *J. Am. Chem. Soc.*, 130(2), pp. 410–411, 2008.

[10] Jennifer C.X., Hunter, G.W., Lukco, D., Liu, C.C., Ward, B.J., Novel Carbon Dioxide Microsensor Based on Tin Oxide Nanomaterial Doped With Copper Oxide. *NASA/TM*, 215436, pp. 1- 2, 2008.

[11] Dubbe, A., Fundamentals of solid state ionic micro gas sensors. *Sensors and Actuators B* , 88, pp. 138–148, 2003.

[12] Suzuki, H., Microfabrication of chemical sensors and biosensors for environmental monitoring. *Materials Science and Engineering C,* 12, pp. 55–61, 2000.

[13] Jimenez-Jorquera, C., Orozco, J., Baldi, A., ISFET Based Microsensors for Environmental Monitoring. *Sensors,* 10, pp. 61-83, 2010.

[14] Lamaka, S.V., Karavai, O.V., Bastos, A.C., Zheludkevich, M.L., Ferreira, M.G.S., Monitoring local spatial distribution of Mg^{2+}, pH and ionic currents. *Electrochemistry Communications,* 10, pp. 259–262, 2008.

[15] Kricka, L.J., Miniaturization of analytical systems. *Clinical Chemistry,* 44(9), pp. 2008–2014, 1998.

[16] Arida H., Joachim P., Michael J., Novel organic membrane based thin-film microsensors for the determination of heavy metal cations. *Sensors*, 6, pp. 435-444, 2006.

[17]   Arida H., Development of a Long-Term Stable Organic Membrane Based Thin-Film Microsensor using New-Type Substrate Surface Treatment. *Talanta*, 71, pp. 1856-1860, 2007.

[18] [Arida H., Monika T., David R., Michael J., A novel thin-film array based on an organic/inorganic sensor hybrid: Microfabrication, characterization and flow-injection analysis application. *Electroanalysis*, 21(10), pp. 1145–1151, 2009.

[19] Arida H., Mohsen Q., Michael J., Microfabrication, characterization and analytical application of a new thin-film silver microsensor. *Electrochimica Acta*, 54, pp. 3543–3547, 2009.

[20] Malinowska, E., Brzózka, Z., Kasiura, K., Egberink, R. J. M., Reinhoudt, D.N. , Lead selective electrodes based on thioamide functionalized calix[4]arenes as ionophores. *Analytica Chimica Acta*, 289, pp. 253- 258, 1994.

[21] Umezawa, Y., Bühlmann, P., Umezawa, K., Tohda, K., Amemiya, S. , *Pure Applied Chemistry*, 72, pp. 1851, (2000).

[22] Mourzina, Y., Schöning, M.J. , Schubert, J. , Zander, W., Legin, A., Vlasov, Y., Kordos, P., Lüth, H., *Sensors and Actuators B*, 71, pp. 13, 2000.

[23] Kloock, J., Mourzina, Y., Ermolenko, Y., Doll, T., Schubert, J., Schöning, M.J., *Sensors*, 4, 156, 2004.

[24] Kloock, J., Mourzina, Y., Schubert, J., Schöning, M.J., *Sensors*, 2, pp. 356, 2002.